Lipophilic Prodrug Charge Masking- insights into new method of peptide prodrugs synthesis conception

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BACKGROUND

Lipophilic Prodrug Charge Masking (LPCM) strategy was first described in 2018 by Schumacher et al.¹ as an answer to a growing need of peptide drugs oral delivery. In short, LPCM assumes transitional masking of hydrophilic peptides' charge (especially those having positively charged residues such as Arg, Lys, and free amino terminus, as well as His or Trp in their sequence) by lipophilic moieties (alkoxycarbonyl) connected by a cleavable bond. The resultant prodrug displays improved intestinal permeability in compare to mother peptide. Once it gets into the systemic blood circulation the lipophilic moiety is cleaved by the serum esterases (mainly CES), and a free active peptide is released. Initial studies proved better permeability and, thus, enhanced oral bioavailability of cyclic model prodrug hexapeptides containing RGD motif. prodrug with masked This outcome encouraged us to look closer to LPCM as a method to transform peptides **APICAL MEMBRANE** MMMMMMMMM into bioavailable drugs. We intended verify its to **HIGH PERMEABILITY** LOW PERMEABILITY **EPITHELIAL CELLS** application to commonly known and applied peptide drugs with proved biological **BASOLATERAL MEMBRANE** activity, i.e. vasopressin and desmopressin **BLOOD STREAM** enzymes

OBJECTIVES

We synthesized series of vasopressin (AVP) and desmopressin (DVP) prodrugs with masked charged in the Nterminus (in case of AVP) or on Arg/D-Arg side chain. Masking groups were various alkoxycarbonyl moieties differing in the alkyl chain length, bearing from 1 to 12 C atoms. The challenging modification of guanidinium group was described in our paper 2 .

Obtained analogues permeability was examined using PAMPA test. We also incubated one of the DVP prudrugs (DVP(Hoc)) in rat serum to confirm its tranformation to unmodified peptide (DVP).





Masking group **R-**(\mathbf{n}' R- is alkyl chain Following alkoxycarbonyl groups were introduced: Et-etyloxycarbonyl, **Prop**-propyloxycarbonyl, MeOEt-2-methoxyethyloxycarbonyl,

RESULTS

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PAMPA tests

compound	permeability P _e (10 ⁻⁶ cm/s)	Log Pe	Mass retention	compound	permeability P _e (10 ⁻⁶ cm/s)	Log Pe	Mass retention	
caffeine	22	-5.01	26%	caffeine	33.80	-4.48	18.69%	
atenolol	1.24	-6.22	12%	atenolol	2.80	-5.66	0.10%	
AVP	5.15	-5.86	4%	DVP	1.24	-5.95	2.73%	
Et-AVP	3.62	-5.67	58%	DVP(Et)	4.21	-3.48	9.77%	
Prop-AVP	2.48	-5.84	41%	DVP(Prop)	4.77	-5.32	10.37%	
But-AVP	5.36	-5.63	57%	DVP(But)	7.78	-5.11	9.32%	
Hoc-AVP	4.26	-5.32	40%	DVP(Hoc)	4.21	-4.97	23%	
Oct-AVP	0*	-	58%*	DVP(Hoc) ₂	116*	-3.88	82.92%	
Dec-AVP	14.76	-4.88	80%	DVP(Oct)	53.5*	-4.28	61.15%	
Dod-AVP	53.10	-4.32	81%					
AVP(Prop) ₂	1.27*	-5.99	37%*	atenolol– low perme	eability marker; eability marker:			
AVP(But) ₂	0.41*	-6.39	53%		,, ,, ,, ,			
*results unreliable; compound in the acceptor at the limit of				High permeability > 4.0 × 10⁻⁶ cm/s ; (in Caco-2 convention, according to Corning [®])				

DVP(Hoc) prodrug to drug DVP conversion in rat serum



 \succ Rapid, within 30min, of DVP conversion prodrug into mother peptide. DVP stable for at least

Davia	RAT SERUM	PRODRUG		
	SIGNAL	DVP(Hoc)		

24 h



METHODS

Synthesis

side;

Peptides were synthesized using Fmoc chemistry on Prelude Peptide Synthesizer (Protein Technology, Inc., USA). Each peptide was synthesized on Rink Amide resin (loading 0.646 mmol/g, GL Biochem Shanghai). The protected derivatives of all Fmoc-amino acids were purchased from different commercial sources. The peptide chain was elongated in the consecutive cycles of deprotection and coupling. Deprotection was performed with 20% piperidine in DMF, and peptide chains elongation was performed using 3-fold molar excess of each Fmoc-protected amino acid, TBTU/HOBt/NMM (molar ratio 1:1:1:2). After completing the synthesis, peptides were cleaved from the resin and the protecting groups were removed in a one-step procedure using a mixture of TFA:phenol:triisopropylsilane: H_2O (88:5:2:5, v/v/v/v). Subsequently, the disulfide bridge was formed using a 0.1 M methanolic iodine solution.

Masking groups were introduced using corresponding alkyl chloroformates. In case of masking N-terminal amine group protection was intorduced on resin, using alkyl chloroformate and DIPEA (molar ratio 1:2) in DMF, reaction time 1-20h. Coupling was repeated until negativ chloranil test. D-Arg side chain was masked in solution. In short, eptide with formed disulphide bridge was dissolved in ACN/H_2O , 2.4 eq of DIPEA was added and cooled down to 0°C, later 1.2 eq of alkyl chloroformate in ACN was added dropwise. Reaction was monitored on HPLC and completed within 1h. Introduction of two masking groups on Arg/D-Arg side chain was more challanging and required preparation of Arg builduing blocks, as described in ².

Obtained crude compunds were purified by reverse-phase high performance liquid chromatography (RP-HPLC) on PLC 2050 Gilson HPLC with Gilson Glider Prep. Software (Gilson, France), equipped with Grace Vydac C18 (218TP) HPLC column (22 × 250 mm, 10 μm, 300 Å, Resolution Systems). The solvent systems were 0.1% TFA (A) and 80% acetonitrile in A (B). The purity of each peptide was checked by RP-HPLC on a Shimadzu Prominence-I LC-2050C 3D equipped with a Kinetex XB-C18 column (150 × 4.6 mm, 5 μm) and a UV-Vis detector. A linear gradient from 10% to 90% B for 20 min, flow rate 1 mL min⁻¹, and detection at 214 nm was used. The mass spectrometry analysis of the synthesized compounds was carried out on MALDI MS (Autoflex maX MALDI-TOF spectrometer, Bruker Daltonics, Germany) using an α-cyano-4-hydroxycinnamic

CONCLUSIONS AND FUTURE PERSPECTIVES

- \checkmark Unmodified AVP shows good permeability P_e 5.15 x 10⁻⁶ cm/s
- \checkmark But-AVP P_e was only slightly better than that of AVP, but mass retention was 14 times higher;
- ✓ P_e for AVP analogues with longest alikyl chains (Dec- and Dod-AVP) are very high (almost 3 and 10 times higher) than for AVP), but their concentration in the acceptor well was very low, on the detection limit;
- ✓ Most compounds are characterized by high mass retention, which suggests that they stay attached to the membrane, as their concentration in the donor well decreases;
- \checkmark We improved DVP permeability (about 3-fold) when Et, Prop or Hoc groups were introduced on D-Arg side chain, while over 6 – fold improvement was observed in case of DVP(But) prodrug;
- ✓ We proved that prodrug (DVP(Hoc)) is rapidly transformed in Rat Serum to active, unmodified peptide drug DVP within 30 min of incubation;
- DVP and its most promising prodrugs (DVP(Et)), (DVP(Prop)), (DVP(But)), (DVP(Hoc)), will be tested on Caco-2 cell model;
- \succ Activity of DVP prodrug showing the highest P_{app} will be examined and compared to unmodified DVP in in vivo

acid and/or 2,5-dihydroxybenzoic acid matrix.

PAMPA Caco-2 convention

Donor well

compound

Artificial

Buffer

well

solution

Acceptor

membrane

Test

PAMPA

PAMPA test was performed according to provider (Corning®)

qauntification, although its concentration decreased in the donnor

instructions.

Experiment conditions:

Caco-2 convention (top well is donor well)

- Buffer: PBS pH 7.4
- Incubation: 25 °C, 22h,

Sample concentration: 10 μ M (AVP assay) and 50 μ M (DVP assay) Plates: Corning® Gentest Pre-coated PAMPA Plate System

- membrane construction: lipid-oil-lipid trilayer; hexane was used to disperse the contents of layers; The **oil layer** mimics the hydrophobic interior of the biological membrane and allows the amphiphilic lipids to anchor on it and is crucial for maintaining a robust and stable artificial membrane. Lipid layer is mixture of phospholipids.

The concentrations of the tested compounds in each well of the acceptor and donor plates were determined by LC-MS technique. The analysis was conducted by UHPLC-MS system (Shimadzu Nexera X2 with LCMS-2020 detector) using a ReproSil Pure 120 ODS-3 column (Dr. Maisch GmbH, 100×2 mm, 2.4 µm particle size) with several gradients of ACN with 0.1% FA and 0.05% TFA at a flow rate of 0.3 mL/min. The eluted solution was monitored by ESI-MS detector operated in the positive ionization mode with the use of the select ion monitoring mode (SIM).

assay;

REFERENCES

1. Schumacher-Klinger A., et al., Enhancing Oral Bioavailability of Cyclic RGD Hexa-peptides by the Lipophilic Prodrug Charge Masking Approach: Redirection of Peptide Intestinal Permeability from a Paracellular to Transcellular Pathway, Mol. Pharm., 2018, 15, 3468-3477. 2. Glavaš M., et al. Synthesis of Novel Arginine Building Blocks with Increased Lipophilicity Compatible with Solid-Phase Peptide Synthesis, Molecules, 2023, 28, 7780.



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